

1 A preliminary investigation into a qualitative  
2 assessment tool to identify athletes with high knee  
3 abduction moments during cutting: Cutting  
4 Movement Assessment Score (CMAS).

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23 Summary

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Given the limited accessibility of 3D motion analysis for injury screening of athletes, there is a need to develop a field-based screening tool to identify athletes with ‘at-risk’ cutting mechanics. The aim of this preliminary study was to assess the validity of a qualitative assessment tool for cutting (CMAS) to estimate the magnitude of peak knee abduction moments (KAM) against ‘Gold Standard’ 3D motion analysis. The presented CMAS was able to rank cutting trials based on the magnitude of KAM. Thus, is a potential method to identify athletes who generate high KAM during cutting.

**Keywords:** Anterior Cruciate Ligament; Knee Abduction Moments; Injury Screening

## 51 Introduction

52 Cutting is an action often associated with non-contact ACL injuries in field and court  
53 based sports such as soccer [4] and handball [23]. This is due to the propensity of generating  
54 high knee abduction (valgus) and rotational moments when the foot is planted [17], which  
55 could lead to increased ACL strain [24, 25]. Whilst the efficacy of screening tests to identify  
56 ‘at-risk’ athletes for specific injuries is debated [1], it is important as strength and  
57 conditioning coaches and sports rehabilitators to have a battery of assessments to provide an  
58 ‘injury profile’ of an athlete. If an athlete underachieves in certain related qualities, steps can  
59 be taken in training to address these deficiencies to provide an overall more rounded and  
60 robust athlete. It is unlikely that one single factor can predict injury alone [1]. Part of such a  
61 battery of assessments with regard to non-contact ACL injuries, should include some  
62 assessment of movement quality during relevant sports actions. In regard to non-contact ACL  
63 injuries, identifying athletes with poor lower limb mechanics in sports where there are large  
64 weight acceptance (braking) forces can be considered important.

65 To date, most literature has examined landing tasks such as the drop jump to identify  
66 ‘at-risk’ athletes despite some sports (i.e., soccer) reporting cutting or changing direction to  
67 be the most common action associated with non-contact ACL injury in females[4]. Hewitt *et*  
68 *al.*, [6] using 3D motion analysis prospectively found that females who went on to injure their  
69 ACL had significantly greater knee abduction angles and moments during a drop jump than  
70 non-injured volleyball players. Although more recent research [15] found such an approach  
71 was unable to identify at-risk athletes for ACL injury in elite soccer and handball players;  
72 which questions the efficacy of the approach to find ‘at-risk’ athletes, but may also suggest  
73 that the screening task needs to reflect the movement demands of the sport. Nevertheless, the  
74 accessibility, time and financial costs will limit the widespread application of 3-Dimensional  
75 analysis to find athletes with poor movement quality, which has led authors to suggest the use

76 of simplified 2D analysis of drop jumps focusing on estimates of frontal plane knee motion  
77 [19, 29]. Moreover, Padua *et al.* [20] have developed and validated a qualitative analysis tool  
78 for a drop jump involving 2D video capture in the frontal and sagittal planes. Although,  
79 mixed evidence has been reported with regard to the efficacy of the Landing Error Scoring  
80 System (LESS) [26, 21] to prospectively predict ACL injury. This may suggest that the use of  
81 landing tasks may fail to identify athletes with at-risk cutting mechanics. Furthermore, there  
82 is also mixed evidence available to suggest whether examination of landing mechanics could  
83 identify athletes with poor cutting mechanics [9,13]. For instance, it is suggested that landing  
84 tasks maybe better at identifying athletes with poor knee control during cutting, but the  
85 ability to identify athletes with high KAMs during cutting from landing is more difficult due  
86 to the differing technical demands of each task [9]. Thus, it is likely that assessment of  
87 movement quality of cutting alongside landing mechanics is needed to further develop the  
88 injury profile of an athlete in cutting and landing sports.

89         Field-based measures evaluating cutting mechanics have also relied on 2D estimates  
90 of frontal plane knee motion. McLean *et al.* [18] investigated whether a 2D assessment of  
91 knee valgus motion relates to knee valgus motion identified from 3D analysis during a 35-60°  
92 side-step, side-jump and shuttle-run (180° turn). 2D estimates correlated well with 3D data  
93 for the side-step ( $R^2 = 0.58$ ) and side-jump ( $R^2 = 0.64$ ), but did not correlate with the shuttle-  
94 run, highlighting the difficulty in assessing knee valgus motion 2-dimensionally in the frontal  
95 plane with more vigorous horizontal changes of direction. Furthermore, such a method only  
96 examines knee valgus motion and does not evaluate the range of technical factors that are  
97 associated with high KAM [3, 8,10,11,12, 17, 27]. Hence, a qualitative screening tool that  
98 examines many aspects of poor cutting mechanics maybe more informative for practitioners.  
99 Therefore, the aim of this preliminary study is to assess the validity of a qualitative screening

100 tool for cutting (Cutting Movement Assessment Score) to estimate the potential magnitude of  
101 KAMs against the ‘Gold Standard’ 3D motion analysis.

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## 103 Methods

### 104 *Participants*

105 With institutional ethical approval, 8 University level team (mean  $\pm$  SD; age: 20.1  $\pm$ 1.1  
106 years, height: 1.63  $\pm$  0.09 m, mass: 54.0  $\pm$  6.9 kg) sport female athletes participated in this  
107 study. For inclusion in the study, all athletes had played their respective sport for a minimum  
108 of 5 years and regularly performed 1 game and 2 structured skill based sessions per week. All  
109 players were right leg dominant. All players were free from injury during the course of the  
110 study and none of the player’s had suffered prior traumatic knee injury such as anterior  
111 cruciate ligament injury. Data collection took place during the players pre-season. Written  
112 informed consent was provided by all subjects.

### 113 Cutting Movement Assessment Score

114 Table 1 presents a qualitative technique analysis tool to estimate the magnitude of  
115 KAMs during cutting (Cutting Movement Assessment Score - CMAS) based on research  
116 pertaining to technique determinants of KAM during 45-90° cutting. If an athlete during  
117 cutting exhibits any of the characteristics in Table 1 they are awarded a score. It is  
118 hypothesised that the greater the total score the greater the potential magnitude of KAM.

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124 **Table 1. A qualitative technique analysis tool to determine the magnitude of knee**  
 125 **abduction moments during cutting – Cutting Movement Assessment Score (CMAS).**

<b>Variable</b>	<b>Observation</b>	<b>Score</b>
<b><u>Penultimate contact</u></b>		
Backward inclination of the trunk	Y/N	Y=0/ N=1
<b><u>Final Contact</u></b>		
Wide lateral leg plant	Y/N	Y=2/N=0
Hip in an initial internally rotated position	Y/N	Y=1/N=0
Initial knee ‘valgus’ position	Y/N	Y=1/N=0
Inwardly rotated foot position	Y/N	Y=1/N=0
Frontal plane trunk position relative to intended direction; Lateral (L), Upright (U) or Medial (M).	L/U/M	L=2/U = 1/M=0
Trunk upright or leaning back throughout contact	Y/N	Y=1/N=0
Limited Knee Flexion during final contact	Y/N	Y=1/N=0
Excessive Knee ‘valgus’ motion during contact	Y/N	Y=1/N=0
	<b>Total Score</b>	<b>/11</b>

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127           The CMAS examines both the penultimate and final contact during the cutting tasks.  
 128 For penultimate contact a ‘backward inclination of the trunk relative to the planted foot’ is  
 129 considered in order to increase horizontal braking forces during penultimate contact, based on  
 130 research [11] that has found an association between average horizontal ground reaction forces  
 131 (GRF) during penultimate contact and KAMs during final contact. For the final contact,  
 132 ‘wide lateral leg plant’ and ‘frontal plane trunk position’ are considered major determinants  
 133 of KAMs [3, 8, 12, 10]; and thus, are given a greater weighting. Previous research has found  
 134 that a wide-lateral foot plant is associated with high KAMs [3, 27, 12, 10] as such a technical  
 135 characteristic may create a GRF vector acting laterally outside the knee with greater distances  
 136 of foot plant creating a greater moment arm and thus, KAM. Lateral trunk flexion has also  
 137 been associated with increasing KAMs during cutting [3, 8, 12, 10], as a laterally flexed trunk

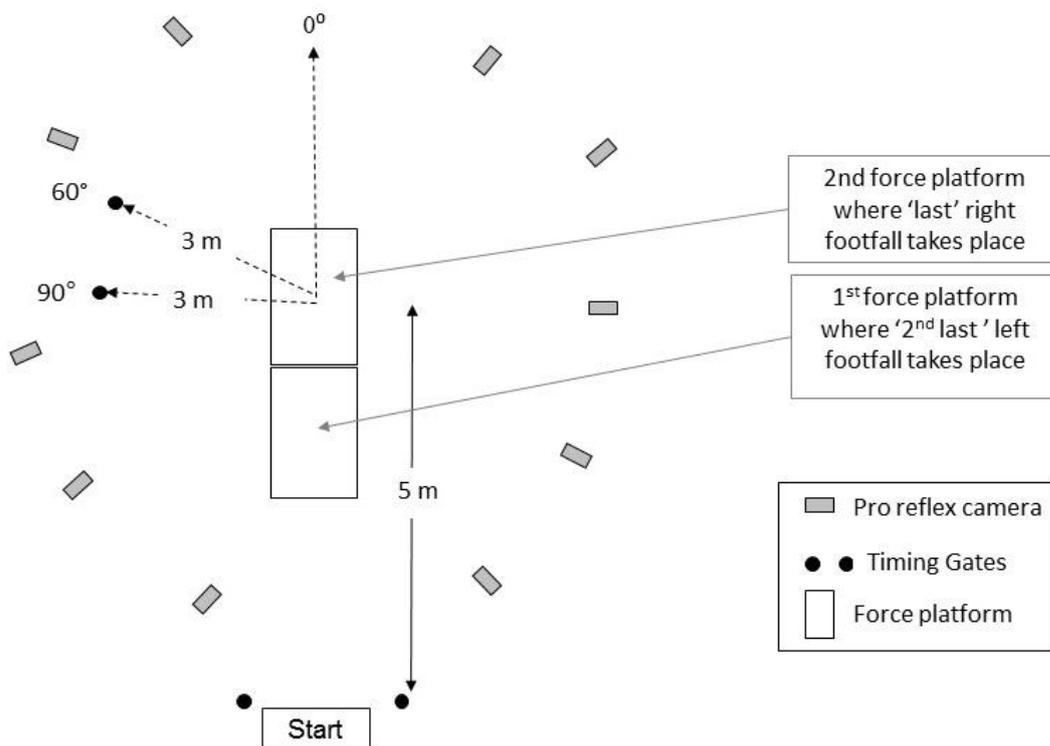
138 towards the planted leg side shifts the athletes weight laterally creating a laterally directed  
139 force vector, increasing the moment arm relative to the knee joint and thus, KAMs.  
140 Other considerations for the final foot contact include ‘initial knee valgus position’, which  
141 has been found in several studies to be associated with KAMs [17, 12, 10]. An increased knee  
142 abduction angle at initial contact has an effect of placing the knee more medial to the  
143 resultant GRF vector and thus, increases the lever arm of the resultant GRF vector relative to  
144 the knee joint leading to an increased KAM. Furthermore, Sigward and Powers [27] found  
145 both initial foot progression angle and initial hip internal rotation angle were significantly  
146 related to KAMs, as such a position could lead to a more medially positioned knee in relation  
147 to the GRF vector [27] and thus, are both considered within the tool. Finally, overall knee  
148 valgus motion during final contact and trunk inclination throughout final contact, with the  
149 latter considered to potentially increase the overall knee joint load due an increased lever arm  
150 of the trunk relative to the knee.

### 151 *Experimental Procedures*

152 The procedures are similar to the methods of Jones et al. [10] and are summarised here. Prior  
153 to data collection, reflective markers (14 mm spheres) were placed on bony landmarks of  
154 each athlete [10], along with 4 marker ‘cluster sets’ (lightweight plastic shell) placed on the  
155 upper back, both thighs and shanks, which approximated the motion of the segments during  
156 dynamic trials.

157 Following a static trial, each athlete performed 5 trials of a between 60-90° cutting task  
158 (Figure 1) which involved sprinting through a set of timing gates (Brower, Draper, UT)  
159 positioned at hip height 5 m from the centre of the plate and then after contacting the centre  
160 of the force platform with the right foot cut to the left through a second set of timing gates  
161 positioned 3 m away. The performance times were used to monitor performance between

162 trials. For each trial, three-dimensional motion data using 10 Qualisys Oqus 7 infrared  
 163 cameras (240 Hz) operating through Qualisys Track Manager Software v2.8 and ground  
 164 reaction force (GRF) data from two AMTI force platforms (sampling at 1200 Hz) were  
 165 collected. This arrangement allowed data to be collected for both penultimate and final  
 166 contact. Simultaneously, 2 Casio EXF-1 cameras (Casio, Tokyo, Japan) sampling at 30 Hz  
 167 were positioned 5 m away from the force platforms in frontal and sagittal planes. Greater  
 168 video sampling rates could not be used as floodlights would have been required to enhance  
 169 lighting, which would have then impacted on 3D motion data collection. Video footage was  
 170 subsequently viewed in Quintic Biomechanics v26 (Coventry, UK) for qualitative analysis  
 171 using the CMAS (Table 1).



172  
 173 **Figure 1. Plan view of the experimental set-up. The task involves subjects approaching 5**  
 174 **m towards a turning point on the 2<sup>nd</sup> of 2 force platforms. At the turning point, subjects**  
 175 **cut to the left between timing cells positioned 3 m away and 60 to 90° from the original**  
 176 **direction of travel.**

177 A lower extremity and trunk 6 degrees of freedom kinematic model was created for  
178 each participant from the static trial. This model included the trunk, pelvis, thighs, shanks and  
179 feet using Visual 3D software (C-motion, version 3.90.21, Gothenburg, Sweden) and is  
180 described in more detail elsewhere [10]. The local coordinate system was defined at the  
181 proximal joint centre for each segment. The static trial position was designated as the  
182 participant's neutral (anatomical zero) alignment, and subsequent kinematic measures were  
183 related back to this position. KAMs were calculated using an inverse dynamics approach [30]  
184 through Visual3d software (C-motion, version 3.90.21) and represented as external moments.

185 Trials were disqualified if the subjects slid or missed the force platform that went  
186 unnoticed during data collection. This resulted in a total of 36 trials considered acceptable for  
187 both 3D and qualitative video analysis. Trials were time normalised for each participant, with  
188 respect to ground contact time. Initial contact was defined as the instant after ground contact  
189 that the vertical GRF was higher than 20 N and end of contact was defined as the point where  
190 the vertical GRF subsided past 20 N. Joint coordinate and force data were smoothed with a  
191 Butterworth low pass digital filter with cut-off frequencies of 12Hz and 25Hz, respectively.  
192 Cut off frequencies were selected based on a residual analysis [30] and visual inspection of  
193 the data.

194

### 195 *Statistical Analysis*

196 To determine inter and intra-rater reliability, 8 trials (1 from each subject) were  
197 randomly selected by one experimenter. One lead researcher (TD) viewed and graded each  
198 trial on two separate occasions and compared (intra-rater reliability), whilst another lead  
199 researcher (PJ) viewed and graded each trial once and compared to the other lead researcher  
200 (inter-rater reliability). Intra-class correlation co-efficients (ICC) for total score were  
201 determined. For each item within the CMAS and total score, percentage agreements

202 (agreements /agreements + disagreements × 100) and Kappa co-efficients were calculated.  
203 Kappa co-efficients were calculated using the formula;  $K = \frac{\text{Pr}(a) - \text{Pr}(e)}{1 - \text{Pr}(e)}$ , where  
204  $\text{Pr}(a)$  = relative observed agreement between raters;  $\text{Pr}(e)$  = hypothetic probability of chance  
205 agreement, using the observed data to calculate the probabilities of each observer randomly  
206 saying each category [5]. The kappa co-efficient was interpreted based on the following scale  
207 of Landis and Koch [16]: 0.01-0.2 (slight); 0.21-0.4 (fair); 0.41-0.6 (moderate), 0.61-0.8  
208 (good) and 0.81-1.0 (excellent).

209         The relationship between CMAS and the ‘gold standard’ determination of peak KAM  
210 during the final contact of the cutting task from 3D motion analysis for all available trials was  
211 explored using Spearman’s rank correlation due to the non-parametric nature of the  
212 qualitative data. Correlations were evaluated as follows: trivial (0.0-0.09), small (0.10 –  
213 0.29), moderate (0.30 – 0.49), large (0.50 – 0.69), very large (0.70 – 0.89), nearly perfect  
214 (0.90 – 0.99), and perfect (1.0) [7].

215

## 216 Results

217 Moderate to excellent intra- and inter-rater agreement was observed (Table 2). Excellent  
218 intra- and inter-rater ICC for total score was also observed (Intra-rater = 0.922; Inter-rater =  
219 0.913).

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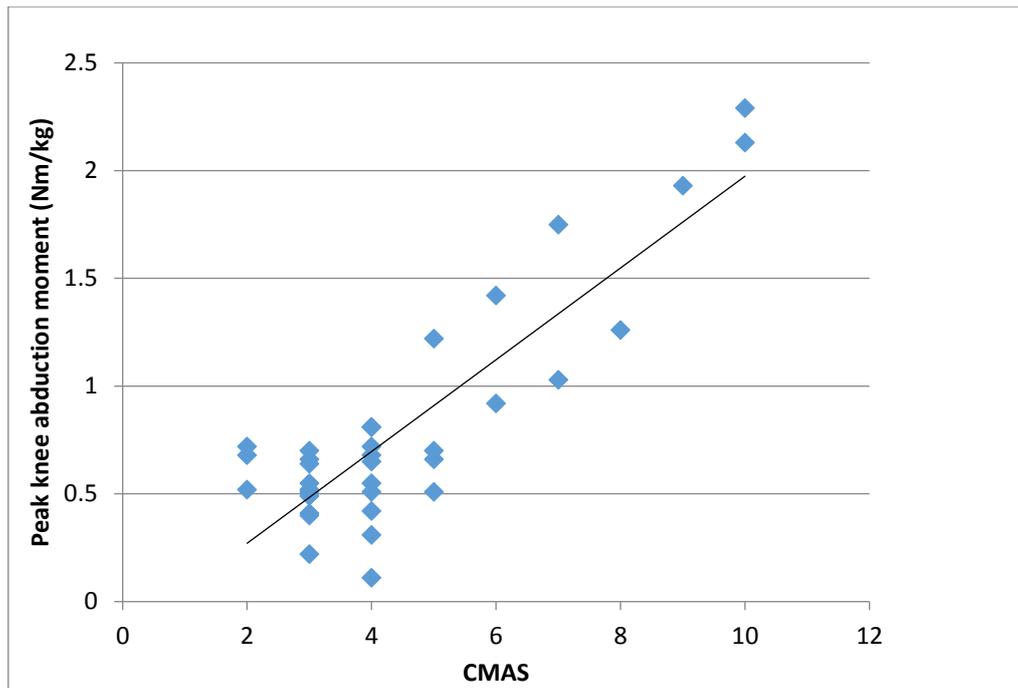
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227 **Table 2. Intra and inter-rater agreement for CMAS criteria and total score.**

Variable/ screening tool criteria	Intra-rater reliability		Inter-rater reliability	
	% Agreement	K	% Agreement	K
Backward inclination of the trunk (penultimate contact)	100	1.00	100	1.00
Wide lateral leg plant	87.5	0.60	100	1.00
Hip in an initial internally rotated position	87.5	0.75	87.5	0.75
Initial knee ‘valgus’ position	87.5	0.60	100	1.00
Inwardly rotated foot position	100	1.00	100	1.00
Frontal plane trunk position relative to intended direction; Lateral (L), Upright (U) or Medial (M).	75	0.62	62.5	0.40
Trunk upright or leaning back throughout final contact	100	1.00	87.5	0.75
Limited knee flexion during final contact	100	1.00	100	1.00
Excessive knee ‘valgus’ motion during final contact	100	1.00	87.5	0.71
Total	93	0.87	92	0.85

228

229 Figure 2 shows a linear relationship between CMAS and KAM’s. Mean  $\pm$  SD KAM  
 230 from each trial of all 8 subjects and the respective CMAS were  $0.80 \pm 0.52 \text{ Nm}\cdot\text{kg}^{-1}$  and  $4.5$   
 231  $\pm 2.1$ , respectively. Spearman’s correlation revealed a significant large association between  
 232 CMAS and KAMs ( $\rho = 0.633$ ;  $p < 0.001$ ).



233

234 **Figure 2. Scatter plot for the relationship between CMAS with peak knee abduction**  
 235 **moments.**

236

237 Discussion

238 The aim of this preliminary study was to assess the validity of a qualitative movement  
 239 assessment tool for cutting (CMAS) to estimate the potential magnitude of KAMs against the  
 240 ‘Gold Standard’ 3D motion analysis. The preliminary results suggest that the presented  
 241 CMAS was able to rank cutting trials based on the magnitude of KAM. Thus, the CMAS can  
 242 be considered a potential method to identify ‘at-risk’ athletes who generate high KAM during  
 243 cutting and could be used in a battery of assessments for an athlete from ‘cutting’ sports to  
 244 develop an injury profile of the athlete. The CMAS also demonstrated excellent inter and  
 245 intra-rater reliability and agreement.

246 The efficacy and efficiency of injury prevention protocols could be improved  
 247 considerably if they are designed specifically for predetermined at-risk athletes, with defined  
 248 neuromuscular control deficits. Whilst screening for specific injury is difficult [1],

249 practitioners require a battery of tests to develop an athlete profile that provides an  
250 assessment of risk factors that could inform training prescription. Central to such a battery of  
251 tests is an assessment of movement quality that relates to common actions in the sport  
252 associated with non-contact injury. Mixed evidence has been reported regarding the efficacy  
253 of using 3D motion analysis of drop jumping [6,15] to prospectively predict ACL injured  
254 athletes and may be partly explained by the need to assess athletes performing common  
255 actions that are associated with injury and occur frequently in change of directions sports,  
256 rather than just purely focus on landing tasks. Furthermore, 3D motion analysis is difficult to  
257 apply for widespread evaluation of athletes. Whilst relationships have been found with regard  
258 to knee motion between landing and changing direction [9, 13], when considering knee joint  
259 loads, lower or absent relationships have been observed [9, 13]; highlighting the need for  
260 field-based assessments of cutting or change of direction mechanics. Current field-based  
261 measures evaluating change of direction mechanics from 2D video analysis can approximate  
262 frontal plane knee motion for shallow angles of direction change only and have not been  
263 shown to predict knee joint loads [18]. The results of the present study suggest that the  
264 CMAS has potential to identify athletes with ‘at-risk’ cutting mechanics and could be used in  
265 a battery of assessments for an athlete from ‘cutting’ sports to develop an injury profile of the  
266 athlete. The use of the CMAS can specifically identify biomechanical or neuromuscular  
267 control deficits in athletes, which can then be targeted via appropriate training and  
268 conditioning.

269         One benefit of CMAS proposed in this study is that it evaluates an action (cutting)  
270 that is common in many sports such as soccer [2] and netball [28], whereas the drop jump is  
271 seldom performed in isolation during sport, as this action is effectively an assessment of an  
272 athlete’s reactive strength. Furthermore, cutting and change of direction actions have been  
273 associated with non-contact ACL injuries in soccer [4] and handball [23], whereas bilateral

274 landings are associated with non-contact ACL injury in basketball [14]. Thus, the CMAS  
275 proposed in this study may serve well for athlete assessment in sports where cutting and  
276 change of direction actions are common. Further work is required to develop the CMAS  
277 particularly with a greater sample of athletes to determine whether the tool is capable of  
278 discriminating between athletes exhibiting poor to excellent cutting technique. Previous  
279 research using the LESS [21] found that 5 was an optimal cut-off score to identify at-risk  
280 athletes for non-contact ACL injury with 86% sensitivity and 64% specificity. Therefore, a  
281 longitudinal study is required to identify a potential cut-off score for the CMAS to identify  
282 ‘at-risk’ athletes and whether the tool can subsequently predict injury.

283         The present study involved team sport athletes with a range of ability levels,  
284 therefore, research is required to establish whether the tool can discriminate between athletes  
285 of different ability levels. In terms of the method of data collection, the intra- and inter-rater  
286 agreements revealed lower percentage agreements for frontal plane trunk position. This was  
287 partially due to the difficulty in viewing this variable in the frontal plane when athletes have a  
288 slightly rotated trunk or pelvis into the intended direction of travel. The authors recommend  
289 placing an additional camera 45° to the original direction of travel in order to improve the  
290 view of variables in the frontal plane when some level of rotation prior to or at initial contact  
291 of final footfall takes place. A further limitation of this study was that due to the need for  
292 additional lighting and to avoid this impacting the 3D motion capture only 30 Hz video  
293 recordings were gathered. Use of greater sampling rates (>100 Hz) would enable more  
294 precise identification of key instances during cutting manoeuvres and therefore, further  
295 enhance validity and reliability of the CMAS. The authors recommend using greater  
296 sampling frequencies (if available) in practice.

297         Finally, another limitation of the present study is that the intra- and inter-rater  
298 reliability and agreements were based on Biomechanics researchers carrying out the

299 investigation. Further work is required to quantify intra- and inter-rater reliability with a  
300 range of applied practitioners such as strength and conditioning coaches, sports rehabilitators  
301 and physiotherapists to be able to apply the CMAS in the field.

302

### 303 Practical Applications for Strength & Conditioning

304 The large association between KAMs from 3D motion analysis and CMAS found in  
305 the present study support the association of the technique characteristics identified in the  
306 CMAS (Table 1) to KAMs during cutting, and therefore, could also act as a guide for  
307 technique development for athletes where the goal is for injury prevention. A unique aspect  
308 of this study is that technical guidelines for safer cutting are provided where currently there  
309 are no guidelines available on how to safely cut. This tool offers a template to enable  
310 practitioners to coach safer cutting technique. However, it should be highlighted that some of  
311 these technique aspects may be detrimental to performance. For instance, a wide lateral foot  
312 plant may facilitate the direction change by helping to generate medial GRF's, but would  
313 result in an initial increase in KAM. Further research is required to better understand the  
314 conflict between performance and injury risk for cutting, which may further inform the  
315 CMAS presented here.

316 A note of caution in using the CMAS is that practitioners should not only focus on  
317 total score but the actual criteria where the athlete scored points. A low score doesn't  
318 necessarily mean that a player has perfect and safe technique. For example, an athlete may  
319 only score two points on the CMAS, however, this score maybe for lateral trunk flexion,  
320 which has been stated as one of the theories of increased risk of ACL injury [22], as such this  
321 deficit in trunk control displayed by an athlete should not be ignored and the athlete should  
322 still receive specific training and conditioning.

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326

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