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4	Validation of the RunScribe Inertial Measurement Unit for walking gait measurement
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21 Abstract

- 22 Intro: The use of portable gait measurement systems in research is appealing to collect real-world
- 23 data at low-cost, low participant burden, and without requirement for dedicated lab space. Most
- 24 commercially available inertial measurement units (IMU's) designed for running only capture
- temporospatial data, the ability to capture biomechanics data such as shock and motion metrics
- 26 with the RunScribe IMU makes it the closest to a lab alternative. The RunScribe system has been
- 27 validated in running, however, is yet to be validated for walking.
- 28 Method: Qualisys motion capture, AMTI force plates, and Delsys Trigno accelerometers were used as
- 29 gold standard lab measures for comparison against the RunScribe IMU. Twenty participants
- 30 completed 10 footsteps per foot (20 total) measured by both systems simultaneously. Variables for
- 31 validation included: Vertical Ground reaction force (GRF), instantaneous GRF rate, pronation
- 32 excursion, pronation velocity, total shock, impact force, braking force. Interclass correlation (ICC)
- 33 was used to determine agreement between the measurement systems, mean differences were used
- 34 to evaluate group level accuracy.
- 35 Results: ICC results showed moderate agreement between measurement systems when both limbs
- 36 were averaged. The greatest agreement was seen for GRF rate, pronation excursion, and pronation
- 37 velocity (ICC = 0.627, 0.616, 0.539), low agreement was seen for GRF, total shock, impact shock,
- braking shock (ICC = 0.269, 0.351, 0.244, 0.180). However mean differences show the greatest level
 of accuracy for GRF, GRF rate, and impact shock.
- 40 Discussion: Results show mixed agreement between the RunScribe and gold standard lab measures,
- 41 and varied agreement across left and right limbs. Kinematic variables showed the greatest
- 42 agreement, however GRF had the lowest relative mean difference for group results. The results
- 43 show acceptable levels of agreement for most variables, however further work must be done to

44 assess the repeatability and sensitivity of the RunScribe to be applied within areas such as footwear

45 testing and gait retraining protocols.

46 Introduction

Gait studies were traditionally undertaken in gait laboratories that require a dedicated space and 47 48 expensive and technically complex measurement devices including motion capture, force platforms, accelerometers, and electromyography (EMG) as key examples. The possibility to collect data in real-49 50 world contexts is attractive because it avoids some of these challenges, especially given the impact of the covid-19 pandemic on research facilities. It also avoids other important pitfalls of laboratory-51 52 based gait studies. Laboratory studies can be a burden to participants who need to be in a set 53 location at a specific date/time which can be a disincentive to participation. It also avoids the 54 influence that researcher presence is known to have on the validity of natural gait during lab-based data collection [1]. Finally, laboratory data requires post-processing which can be time consuming 55 and delay access to results and slow subsequent decision making. 56 57 Gait data collected outside of a laboratory setting has arguably far greater external validity as it 58 allows for a more natural gait to be captured and continuous data collection over a longer period of time than laboratory studies allow [2]. The opportunity therefore arises for studies that once took 59 60 place in laboratory settings to now be undertaken with greater external validity through use of 61 portable measurement systems, as long as such systems accurately measure the pertinent variables. Testing of footwear and foot orthoses in terms of their impact on ground reaction forces, foot 62 63 motion, especially pronation, and "shock", have occupied many researchers where a holistic 64 approach of gait characterisation commonly requires laboratory-based study [3,4]. The ability to transfer objective orthotic testing from a lab into the real world is therefore attractive, with many 65 66 factors working in the favour of portability, including cost, space, availability, and application within 67 participants.

68	This notion has led to development of hardware enabling out of lab data collection, with
69	development of portable systems for gait measurement [5] and measurement of temporospatial gait
70	parameters on different outdoor surfaces [6]. This has facilitated data collections such as the
71	comparison of gait in healthy individuals and Parkinson's patients whereby participants used
72	measurement systems in their daily life for 7 days [7]. Many wearable sensor systems focus on
73	measurement of temporospatial gait parameters, targeted towards recreational runners and their
74	running performances and habits (e.g. ARION, NURVV, Stryd, GWalk, RunScribe). Common gait
75	parameters include step length, stride length, contact time, speed, pace, distance, and duration.
76	Previous study has shown good levels of agreement for the Stryd (ICC > 0.81) when compared to
77	high-speed video for contact time, flight time, step frequency, and step length during running [8].
78	Comparison against an OptoGait gait measurement system at different running speeds showed high
79	ICC values for step length (>0.934) and step frequency (>0.956), however agreement was lower for
80	contact time (<0.463) and flight time (0.555 – 0.806) [9]. When compared to a motion capture
81	system, measures of ground contact time and leg spring stiffness measured by the Stryd were
82	deemed acceptable [10]. The GWalk has shown good reliability for speed, cadence, stride duration
83	and stride length (rho > 0.75) in comparisons against an instrumented carpet [11], and high ICC
84	values (> 0.728) have also been seen in test-retest reliability analyses of a range of gait parameters
85	measured by the GWalk [12]. The RunScribe IMU perhaps provides the most in-depth analysis of all
86	these units, offering measurement including pronation excursion, pronation velocity, impact shock,
87	braking shock, total shock ground reaction force (GRF), and GRF rate. Validation studies have only
88	focused on pronation variables at running speeds where agreement with a 3D motion system was
89	very mixed (Pronation Excursion (ICC = $0.4 - 0.57$), Pronation Velocity (ICC = $0.74 - 0.87$)) [13], and
90	running shock in different footwear conditions with low correlation between the RunScribe and
91	tibial accelerometer (r = 0.42) and between the RunScribe and a shoe mounted accelerometer (r = $(r = 1)$
92	0.57) [14]. A more inferential study demonstrated that the RunScribe shock variables were

significantly different between surfaces (P=0.001) and speeds (P<0.001) indicating the ability for the
RunScribe to detect change between conditions [15].

The RunScribe IMU is the most rounded wearable gait measurement device with a range of 95 96 biomechanical variables relevant for human gait measurement including pronation excursion, 97 pronation velocity, ground reaction force (GRF), GRF rate, impact shock, braking shock, and total shock in addition to temporospatial gait parameters. Pronation and shock variables are measured 98 directly by the RunScribe unit and system, however GRF parameters are estimated using equations 99 100 utilising contact time and flight time measured by the RunScribe, these equations were defined in 101 previous research on middle distance runners [16]. In comparison to other units, the RunScribe 102 provides measurement of variables pertinent to footwear and orthotic testing, and the design of orthoses. Therefore validating the RunScribe IMU to ensure the unit provides accurate and reliable 103 measures of these variables during walking would enable the advancement of externally valid 104 105 testing of footwear and orthotic products. Footwear testing that once took place in laboratory 106 settings could be undertaken in real-world settings with greater external validity.

107 Aims & Hypothesis

108 The aims of the current study were to assess the accuracy of the RunScribe IMU against Gold 109 standard biomechanics laboratory-based measurements of the data it provides on ground reaction 110 forces, foot kinematics, and shock. It is hypothesised that agreement will be mixed across all 111 variables and that pronation and shock variables will show the greatest level of agreement to the 112 gold standard lab measures due to the direct measurement of these variables, agreement will be 113 lower for force variables due to inference of these variables. However, methodological constraints 114 may reduce accuracy of the shock variables as measured by the RunScribe system compared to the 115 laboratory-based measurement of the shock variables due to the placement of the RunScribe on the 116 foot, and the laboratory sensor on the shank.

117 Methods

- 118 Twenty Participants (Male n = 8, Female n = 12) took part in the testing: Age (33.6 ± 10.6 Years),
- 119 Height (170.9 ± 7.8 cm), Body Mass (73.2 ± 11.9 Kg). Ethical clearance for the protocol was granted
- 120 by The University of Salford ethics committee, application number 1391. Written consent was
- 121 obtained from all participants prior to commencement of the research protocol.

122 Gold Standard Lab Measurements

Participants walked at self-selected speed across a laboratory walkway whilst foot kinematics, GRF 123 124 and accelerometer data were collected simultaneously. Two instrumented force plates (AMTI, 125 Massachusetts, USA) operating at 1000 Hz were spaced to allow both plates to be contacted with the same foot. Thirteen Qualisys Oqus cameras (Qualisys, Gothenburg, Sweden) operating at 100 Hz 126 127 were used for 3D motion capture. Marker setup was completed bilaterally as follows: Medial knee, 128 Lateral Knee, Medial Malleolus, Lateral Malleolus, Heel, MH1, MH2, MH5, with the addition of a 4 129 marker cluster on the outer shank (Fig 1). A Delsys Trigno Avanti (Delsys, Natick, Massachusetts, USA) unit sampling at 135Hz was affixed bilaterally to the shank of participants and subsequently 130 131 wrapped using medical tape to fix the accelerometer in place and prevent movement during the protocol. Participants completed 5 walks targeting the force plate with the left foot, and 5 targeting 132 133 with the right foot, resulting in a total of 10 steps per foot for comparison. Participants completed this whilst wearing their own footwear. 134 135 Figure 1. Marker and equipment placement on a) Participant footwear and b) lower limbs.

- 136 Data from force plate contact only was processed using Visual 3D (C-Motion, Maryland, USA) to
- 137 extract GRF (xBW) and peak GRF rate (N/s) from force plate data, and Pronation Excursion (°),
- 138 Maximum pronation velocity (°/sec) from marker-based motion data. Pronation Excursion was
- defined as the amount of pronation from initial contact to maximum pronation, maximum pronation

140	velocity was the maximum instantaneous velocity of joint rotation during this period. A Butterworth
141	low pass filter was used on marker trajectories (10Hz) and force data (20Hz). The shank was
142	modelled using medial and lateral knee markers, shank cluster and medial and lateral malleolus
143	markers. The foot was modelled as a whole using medial and lateral malleolus, heel, and metatarsal
144	head markers. Pronation was defined as the rotation of the foot with respect to the shank in the
145	frontal plane. Peak positive vertical acceleration and peak negative horizontal acceleration was
146	taken from accelerometer data as the impact shock (g) and braking shock (g) respectively and
147	combined in the same manner as the RunScribe to give total shock (g).
148	RunScribe IMU
149	The RunScribe Plus IMU device (500 Hz) (Scribe labs, Moss Beach, California, USA) was fitted to the

RunScribe IMU 148

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149	The RunScribe Plus IMU device (500 Hz) (Scribe labs, Moss Beach, California, USA) was fitted to the
150	laces of both left and right shoes as per the manufacturer instructions (Figure 1) The RunScribe is a
151	commercially available device with a pre-programme algorithm that delivers maximum values of the
152	variables in question per step, rather than delivering the data across the whole time of the gait cycle.
153	The RunScribe system was started manually before each walk across the force plate, and stopped
154	when the individual had passed the force plates. This enabled the steps before and after the steps
155	with force plate contact to be captured by the RunScribe. Individuals approached the force plate in a
156	self-selected manner, the number of steps before the force plate was identified and these steps
157	were used to identify the next two steps as the steps that contacted the force plate. The data could
158	then be extracted from the RunScribe for the relevant steps that contacted the force plates, and
159	then matched to the data for the same footsteps from the gold standard laboratory system post
160	processing. Data was downloaded and the steps matching those used for GRF, kinematic, and
161	acceleration data collection extracted. Variables taken from the RunScribe IMU are detailed in table
162	1.

163 Table 1. Definition of variables measured by the RunScribe Plus IMU.

Variable	RunScribe definition
Pronation Excursion (°)	Amount of rotation from initial foot contact to maximum pronation
Pronation Velocity (°/sec)	Maximum velocity of pronation between initial foot contact and maximum pronation
GRF (xBW)	Peak vertical GRF
GRF Rate (N/Kg/s)	Mean vertical force during stance
Total Shock (g)	Vector combination of impact and braking shock
Impact Shock (g)	Peak positive vertical acceleration
Braking Shock (g)	Peak negative horizontal acceleration

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Data from all systems was collected on the left and right limbs, and a single measure per participant was also created through averaging these scores. All data was included for further analysis to provide insight into repeatability through the differences between the systems in both limbs. The average measure was created to provide a single reference measure for comparison of the two measurement systems.

170 Statistics

171	SPSS statistics 26 (IBM, New York, USA) was used to conduct a two-way mixed effects ICC with
172	average measures and absolute agreement (ICC 3,1) to determine the level of agreement between
173	the RunScribe IMU (RS) and the gold standard lab measures (LAB), the test was completed on left
174	and right data individually, and the averaged data. ICC values are classed as: <0.5 (low), 0.5 - 0.75
175	(moderate), 0.75 – 0.9 (good), 0.9 – 1.0 (excellent) [17]. Mean differences were calculated as LAB
176	minus RS, percentage mean difference was calculated using these mean differences as a percentage
177	of the lab value. Outlying data was consistently present for 2 participants for the GRF rate, and all 3
178	shock variables. These outliers caused the data to be non-normally distributed, the outlying data was

179 subsequently explored however there was no evident reasoning for the outlying data,

180 therefore these outliers were removed from analysis leaving data normally distributed.

181 **Results**

182 Table 2. Comparison of all variables with data from both limbs combined (Mean ± SD), with ICC

183 and mean differences (LAB – RS).

Variable	RS	LAB	ICC	Mean Difference	% Mean
				S	Difference
Pronation Excursion (°)	8.05 ± 3.78	10.07 ± 1.90	0.616	2.02 ± 2.88	20.06
Pronation velocity (°/sec)	229.82 ± 70.16	182.15 ± 41.04	0.539	-47.67 ± 58.22	-26.17
GRF (xBW)	1.16 ± 0.05	1.13 ± 0.04	0.269	-0.03 ± 0.06	-2.62
GRF rate (N/s)	14.12 ± 0.84	14.66 ± 2.40	0.627	0.54 ± 1.87	3.65
Total shock (g)	2.54 ± 0.41	1.79 ± 0.47	0.351	-0.76 ± 0.43	-42.30
Impact shock (g)	1.47 ± 0.37	1.42 ± 0.42	0.244	-0.06 ± 0.52	-3.92
Braking shock (g)	1.94 ± 0.39	1.03 ± 0.37	0.180	-0.92 ± 0.42	-88.90

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185 Data comparing the outcome variables averaged for both limbs is present in Table 2. Moderate

186 levels of agreement between RS and LAB are present for pronation variables. Agreement was low for

187 GRF (0.269), but moderate for GRF rate (0.627). There was also low agreement for all shock

188 variables. Mean differences show GRF, impact shock, and GRF rate to be comparable across systems

with differences of less than $\pm 4\%$. Greater mean differences are present for braking shock, total

190 shock, pronation excursion, and pronation velocity with differences from ± 20.06 – 88.90%

191 Table 3. Comparison of left foot data from all variables (Mean ± SD), with ICC and mean

192 differences (LAB - RS).

Variable	RS	LAB	ICC	Mean Difference	% Mean
					Difference
Pronation Excursion (°)	8.29 ± 4.53	9.84 ± 2.07	0.606	1.55 ± 3.64	15.76
Pronation velocity (°/sec)	221.26 ± 74.76	177.97 ± 40.62	0.510	-43.29 ± 64.72	-24.33
GRF (xBW)	1.16 ± 0.07	1.13 ± 0.04	0.383	-0.03 ± 0.06	-2.74
GRF rate (N/s)	14.13 ± 0.91	14.44 ± 2.66	0.594	0.31 ± 2.15	2.14
Total shock (g)	2.53 ± 0.54	1.86 ± 0.55	0.434	-0.68 ± 0.55	-36.40
Impact shock (g)	1.53 ± 0.40	1.49 ± 0.46	0.474	-0.04 ± 0.51	-2.69
Braking shock (g)	1.88 ± 0.55	1.06 ± 0.43	0.269	-0.83 ± 0.56	78.10

193 Data the outcome variables for the left foot is present in Table 3. Moderate levels of agreement

194 were again seen between the two measurement systems for pronation variables. Agreement was

195 low for GRF (0.383) and moderate for GRF rate (0.594). Agreement was again low but close to

196 moderate for total shock (0.434) and impact shock (0.474), however was low for braking shock

197 (0.269). Data was comparable across systems for GRF rate, GRF, and impact shock with mean

198 differences less than ± 3%. Mean differences from ± 15.76 to 78.10% were present for braking shock,

199 pronation excursion, pronation velocity, and total shock.

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203 Table 4. Comparison of right foot data from all variables (Mean ± SD), with ICC and mean

204 differences (LAB - RS).

Variable	RS	LAB	ICC	Mean Difference	% Mean
				16(2)	Difference
Pronation Excursion (°)	7.82 ± 3.65	10.31 ± 2.48	0.604	2.49 ± 2.92	24.16
Pronation velocity (°/sec)	238.37 ± 76.66	186.32 ± 52.34	0.600	-52.05 ± 62.00	-27.94
GRF (xBW)	1.15 ± 0.05	1.12 ± 0.04	0.092	-0.03 ± 0.06	-2.49
GRF rate (N/s)	14.10 ± 0.81	14.87 ± 2.42	0.579	0.76 ± 1.92	5.12
Total shock (g)	2.55 ± 0.56	1.71 ± 0.46	0.260	-0.84 ± 0.58	-48.70
Impact shock (g)	1.42 ± 0.47	1.35 ± 0.41	0.189	-0.07 ± 0.59	-5.28
Braking shock (g)	2.00 ± 0.51	1.00 ± 0.39	0.115	-1.00 ± 0.57	-100.32

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206	Data comparing systems for the right foot is present in Table 4. Agreement was again moderate in
207	the right limb for pronation variables. Very low agreement was seen for GRF (0.092), and moderate
208	agreement for GRF rate (0.579). Low agreement was again seen for all shock variables (ICC < 0.260).
209	Mean differences show GRF, impact shock, and GRF rate to be comparable across systems with
210	differences less than $\pm 6\%$. Mean differences show less comparable results between systems for
211	pronation excursion, pronation velocity, total shock, and braking shock with differences from \pm 24.16
212	to 100.32%.

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213 Discussion

214 The current study is the first to attempt to validate the RunScribe IMU for use in walking. The 215 comparison to gold standard lab shows mixed levels of agreement. The RunScribe both under-216 estimated and over-estimated variables, however differences apparent within the left and right 217 limbs were always unidirectional. Overall agreement was moderate with some variables with low 218 agreement, kinematic variables showed greater levels of agreement than all other variables. The 219 mean differences also show mixed results, with large relative mean differences for braking shock 220 and low mean differences in GRF. Mean differences also displayed inconsistency within some variables with large differences between left and right limbs. 221

222 GRF data consistently shows the lowest mean difference (-2.49 - -2.74%) of all variables, although 223 agreement was low (ICC = 0.092 - 0.383). Low relative mean differences were also present for the 224 GRF rate data (2.14% – 5.12%), however with greater, moderate levels of agreement (ICC = 0.579 -225 0.627). There were no previous studies attempting to validate these variables as measured by the 226 RunScribe in either walking or running. The GRF data is the only data measured by the RunScribe 227 within the study that is inferred as opposed to directly measured. This may provide evidence for the low levels of agreement seen within these variables. However, the Mean differences were the 228 lowest of all variables within the study. Within lab studies GRF is measured using instrumented force 229 plates, IMU based systems with similar portability of the RunScribe are available for estimates of 230 231 GRF but do not provide a direct measurement of GRF. Systems such as the TekScan F-Scan are 232 available for portable measures of GRF, however this system is bound to some of the same 233 restrictions as a laboratory, with high cost and requirement for additional equipment to log data 234 collected by the system. Application of this type of system is also slightly more burdensome on the 235 participant, due to wires and the data logger which must be with the participant. The group level 236 accuracy and the portable nature of the RunScribe positions the system as an easy to apply measure 237 of GRF, whereby more sophisticated laboratory equipment is required for direct measurement. GRF 238 rate has been used within research studies to show association between cushioning properties 239 present within footwear and reductions in GRF rate [18,19]. Cushioning is a property within

footwear that is highly sought after by a wearer, and is often subjectively related to footwear
comfort [20]. High loading rates have previously been associated with lower limb stress fractures in
runners [21], however this is limited to running and the lower loading rates associated with walking
are not linked to stress injuries.

244 RunScribe shock variables differed in their agreement with the gold standard lab measurement. Impact shock showed the lowest difference between systems (mean differences of -2.69 - -5.28%) 245 however showed low agreement (ICC = 0.189 - 0.474), far better than for braking shock (mean 246 247 differences -78.10 - -100.32% however with similar ICC results (ICC = 0.115 - 0.269). Due to total 248 shock being derived from braking and impact shock it falls between their results in terms of 249 reliability (mean differences -36.40 - -48.70% and ICC = 0.260 - 0.434). A previous study has compared impact shock measures of the RunScribe to peak positive acceleration (PPA) measured at 250 the shank and shoe using an IMeasureU accelerometer showing overall correlation of r=0.46, 251 252 representing a moderate correlation between the reference accelerometer and the RunScribe [14]. Previous findings are consistent with current results whereby the RunScribe measures impact shock 253 to be greater than a traditional IMU mounted on the shank. Reasoning for this difference is 254 evidenced in previous research, which shows movement of the shoe independent of the foot and 255 body can attenuate the shock experienced by the body [22]. Braking shock in the current research 256 257 may be most affected by the notion of uncoupled motion of foot and shank, with the greatest 258 differences present between the RunScribe and gold standard measurement system. During the 259 time of peak impact shock the shank and foot move similarly, however peak braking shock is 260 observed slightly later after foot contact, whereby the foot has experienced severe deceleration and 261 is no longer in motion, whereas the shank has experienced deceleration resulting in a slowing down 262 in forward progression of the shank. Another potential methodological constraint surrounding the 263 Delsys accelerometer in the current investigation is the low sampling rate, using lower sampling 264 rates for acceleration measurement has been associated with data loss within running research, it 265 was however identified that lower sampling frequencies are required for walking speeds to provide

266	accurate results [23]. Shock variables are becoming more prevalent in assessment of running
267	footwear [24,25] and insole products [26,27] with manipulations in both products able to deliver
268	shock absorption. Shock absorbing footwear is frequently posed as a method of injury prevention
269	[28] with shock absorption also contributing to feelings of footwear comfort [29] leading to
270	individuals seeking shock absorption within footwear. The RunScribe therefore has potential uses in
271	footwear assessment in different domains for injury risk and understanding contributions of shock
272	absorption to footwear comfort.
273	Pronation excursion shows moderate agreement (ICC = 0.604 – 0.616) and inconsistent mean
274	differences (15.76% – 24.16%). Pronation velocity also displayed moderate agreement (ICC = 0.510 –
275	0.600) and larger mean differences (-24.33% – 27.94%). The RunScribe pronation variables are the
276	only variables that have previously been compared to gold standard lab measures [13], however this
277	was at running speeds. Agreement was mixed for pronation excursion with moderate agreement in
278	the left limb (ICC = 0.57) but low agreement in the right limb (ICC = 0.40). Mean differences were
279	also mixed, the left limb displayed a mean difference of -4.0° (-27.4%) and the right limb displaying a
280	mean difference of 0.5° (3.6%). Good agreement was seen for pronation velocity in both left (ICC =
281	0.74) and right (ICC = 0.87) limbs, however mean differences were largely varied between limbs.
282	Mean difference was much lower in the left limb at 8.6°/sec (Runscribe 1.9% greater than 3D
283	motion) than in the right limb at 149°/sec (Runscribe 41% greater than 3D motion). Alongside more
284	consistent difference to lab measures, the current results show more promise regarding the
285	unidirectional difference compared to the lab for pronation excursion, with the RunScribe measuring
286	both limbs lower than the lab. Pronation excursion is a key variable for many research studies
287	examining orthotic intervention for reduction of frontal plane motion [30] and relationship between
288	excessive pronation in runners and injury risk for medial tibial stress syndrome [31] and achilles
289	tendinopathy [32]. Therefore, the RunScribe poses as an effective method for assessing this variable
290	with a range of interventions within a real-world environment.

291	The present study has presented a comparison of the RunScribe to lab measures during walking for
292	the first time, the current methodology does however contain some limitations. As previously
293	mentioned, the difference in placement between the two measures of shock may have created
294	some difference in measures resulting from attenuation seen at the shank not present at the foot.
295	Shank mounting of the laboratory IMU was chosen as it is the gold standard for measurement of
296	shock in research studies, therefore this protocol was followed in the current methods as the
297	objectives of the study were to compare the measurements of the RunScribe to a gold standard
298	laboratory system and methodology. Placing the laboratory IMU on the shoe would have provided
299	greater agreement as the measurement systems would have been closer in proximity, however the
300	method would then have been tailored to show greater agreement between the RunScribe and the
301	laboratory system as opposed to reflecting standard approaches. No study to date, including the
302	current study, has compared the repeatability of the RunScribe unit over a number of assessments
303	or days. Further study with repeated measurements to provide more robust measures of accuracy,
304	and proving the repeatability of the system would be key for the implementation of the RunScribe
305	IMU within research testing interventions, and application within footwear or orthotic testing within
306	the real-world environment. The RunScribe has however been previously applied in gait
307	characterisation of healthy and injured runners [33], and a quantification of cumulative shock in
308	runners to inform changes in training load [34]. The RunScribe is beginning to be used as a tool for
309	real-world research, however further research should be completed assessing the sensitivity and
310	repeatability of the RunScribe for the ability to detect differences between different footwear
311	conditions and interventions, but also the ability to detect accurate individual differences within a
312	participant sample.

313 Conclusion

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Current results display moderate agreement between the RunScribe IMU and the gold standard lab
measurements for the majority of the variables. Some variables however show low agreement with

316 traditional gold standard lab measurement. With varied agreement amongst variables, but also 317 varied agreement between limbs the application of the RunScribe must be carefully considered 318 when being used within intervention studies, and the comparison of data across studies. However, 319 there has been emergence of the RunScribe IMU being used as a standalone tool within research in 320 a variety of studies and this study expanded this yet further.

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References 326

327	1.	Friesen, K.B., Zhang, Z., Monaghan, P.G., Oliver, G.D. and Roper, J.A., 2020. All eyes on
328		you: how researcher presence changes the way you walk. Scientific Reports, 10(1), pp.1-8.
329	2.	Benson LC, Clermont CA, Bošnjak E, Ferber R. The use of wearable devices for walking and
330		running gait analysis outside of the lab: A systematic review. Gait & posture. 2018 Jun
331		1;63:124-38.
332	3.	Cheung RT, Wong MY, Ng GY. Effects of motion control footwear on running: a systematic
333		review. Journal of sports sciences. 2011 Sep 1;29(12):1311-9.
334	4.	Hoitz F, Mohr M, Asmussen M, Lam WK, Nigg S, Nigg B. The effects of systematically altered
335		footwear features on biomechanics, injury, performance, and preference in runners of
336		different skill level: a systematic review. Footwear Science. 2020 Sep 1;12(3):193-215.
337	5.	Haque MR, Imtiaz MH, Kwak ST, Sazonov E, Chang YH, Shen X. A Lightweight Exoskeleton-
338		Based Portable Gait Data Collection System. Sensors. 2021 Jan;21(3):781.

339	6.	Kowalsky DB, Rebula JR, Ojeda LV, Adamczyk PG, Kuo AD. Human walking in the real
340		world: Interactions between terrain type, gait parameters, and energy expenditure. PLoS one.
341		2021 Jan 13;16(1):e0228682.
342	7.	Coates L, Shi J, Rochester L, Del Din S, Pantall A. Entropy of real-world gait in Parkinson's
343		disease determined from wearable sensors as a digital marker of altered ambulatory
344		behavior. Sensors. 2020 Jan;20(9):2631.
345	8.	García-Pinillos F, Latorre-Román PÁ, Soto-Hermoso VM, Párraga-Montilla JA, Pantoja-
346		Vallejo A, Ramírez-Campillo R, Roche-Seruendo LE. Agreement between the spatiotemporal
347		gait parameters from two different wearable devices and high-speed video analysis. PLoS
348		One. 2019 Sep 24;14(9):e0222872.
349	9.	García-Pinillos F, Roche-Seruendo LE, Marcén-Cinca N, Marco-Contreras LA, Latorre-
350		Román PA. Absolute reliability and concurrent validity of the Stryd system for the assessment
351		of running stride kinematics at different velocities. The Journal of Strength & Conditioning
352		Research. 2021 Jan 1;35(1):78-84.
353	10.	Imbach F, Candau R, Chailan R, Perrey S. Validity of the Stryd power meter in measuring
354		running parameters at submaximal speeds. Sports. 2020 Jul;8(7):103.
355	11.	Vítečková S, Horáková H, Poláková K, Krupička R, Růžička E, Brožová H. Agreement
356		between the GAITRite® System and the Wearable Sensor BTS G-Walk® for measurement of
357		gait parameters in healthy adults and Parkinson's disease patients. PeerJ. 2020 May
358		22;8:e8835.
359	12.	YAZICI G, YAZICI MV, ÇOBANOĞLU G, KÜPELİ B, OZKUL C, OSKAY D, GÜZEL NA. The
360		reliability of a wearable movement analysis system (G-walk) on gait and jump assessment in
361		healthy adults. Journal of Exercise Therapy and Rehabilitation. 2020;7(2):159-67.
362	13.	Koldenhoven RM, Hertel J. Validation of a wearable sensor for measuring running
363		biomechanics. Digital biomarkers. 2018;2(2):74-8.
364	14.	Napier C, Willy RW, Hannigan BC, McCann R, Menon C. The effect of footwear, running
365		speed, and location on the validity of two commercially available inertial measurement units
366		during running. Frontiers in Sports and Active Living. 2021 Apr 26;3:102.
367	15.	Hollis CR, Koldenhoven RM, Resch JE, Hertel J. Running biomechanics as measured by
368		wearable sensors: effects of speed and surface. Sports biomechanics. 2019 Mar 7.

369	16. Di Michele R. Relationships between running economy and mechanics in middle-distance
370	runners.
371	17. Koo TK, Li MY. A guideline of selecting and reporting intraclass correlation coefficients for
372	reliability research. Journal of chiropractic medicine. 2016 Jun 1;15(2):155-63.
373	18. Logan S, Hunter I, Hopkins JT, Feland JB, Parcell AC. Ground reaction force differences
374	between running shoes, racing flats, and distance spikes in runners. Journal of sports science
375	& medicine. 2010 Mar;9(1):147.
376	19. Soares D, Charalambous L, Rodrigues P, Mitchell A. Effects of Midsole Thickness on Single
377	Leg Drop Landing Ground Reaction Force and Dynamic Stability. ISBS Proceedings Archive.
378	2018;36(1):554.
379	20. Goonetilleke RS. Footwear cushioning: relating objective and subjective measurements.
380	Human factors. 1999 Jun;41(2):241-56.
381	21. Zadpoor AA, Nikooyan AA. The relationship between lower-extremity stress fractures and the
382	ground reaction force: a systematic review. Clinical biomechanics. 2011 Jan 1;26(1):23-8.
383	22. Cheung RT, Zhang JH, Chan ZY, An WW, Au IP, MacPhail A, Davis IS. Shoe-mounted
384	accelerometers should be used with caution in gait retraining. Scandinavian journal of
385	medicine & science in sports. 2019 Jun;29(6):835-42.
386	23. Mitschke C, Zaumseil F, Milani TL. The influence of inertial sensor sampling frequency on the
387	accuracy of measurement parameters in rearfoot running. Computer methods in
388	BiomeChaniCs and BiomediCal engineering. 2017 Oct 26;20(14):1502-11.
389	24. Sinclair J, Greenhalgh A, Brooks D, Edmundson CJ, Hobbs SJ. The influence of barefoot and
390	barefoot-inspired footwear on the kinetics and kinematics of running in comparison to
391	conventional running shoes. Footwear Science. 2013 Mar 1;5(1):45-53.
392	25. Sinclair J. The influence of minimalist, maximalist and conventional footwear on impact shock
393	attenuation during running. Movement & Sport Sciences-Science & Motricité. 2017(95):59-64.
394	26. Lucas-Cuevas AG, Camacho-García A, Llinares R, Priego Quesada JI, Llana-Belloch S,
395	Pérez-Soriano P. Influence of custom-made and prefabricated insoles before and after an
396	intense run. PloS One. 2017 Feb 28;12(2):e0173179.

397	27. Lavender SA, Wang Z, Allread WG, Sommerich CM. Quantifying the effectiveness of static
398	and dynamic insoles in reducing the tibial shock experienced during walking. Applied
399	ergonomics. 2019 Jan 1;74:118-23.
400	28. Bonanno DR, Landorf KB, Munteanu SE, Murley GS, Menz HB. Effectiveness of foot orthoses
401	and shock-absorbing insoles for the prevention of injury: a systematic review and meta-
402	analysis. British journal of sports medicine. 2017 Jan 1;51(2):86-96.
403	29. Silva RM, Rodrigues JL, Pinto VV, Ferreira MJ, Russo R, Pereira CM. Evaluation of shock
404	absorption properties of rubber materials regarding footwear applications. Polymer testing.
405	2009 Sep 1;28(6):642-7.
406	30. Kosonen J, Kulmala JP, Müller E, Avela J. Effects of medially posted insoles on foot and
407	lower limb mechanics across walking and running in overpronating men. Journal of
408	biomechanics. 2017 Mar 21;54:58-63.
409	31. Okunuki T, Koshino Y, Yamanaka M, Tsutsumi K, Igarashi M, Samukawa M, Saitoh H,
410	Tohyama H. Forefoot and hindfoot kinematics in subjects with medial tibial stress syndrome
411	during walking and running. Journal of Orthopaedic Research®. 2019 Apr;37(4):927-32.
412	32. Azevedo LB, Lambert MI, Vaughan CL, O'Connor CM, Schwellnus MP. Biomechanical
413	variables associated with Achilles tendinopathy in runners. British journal of sports medicine.
414	2009 Apr 1;43(4):288-92.
415	33. Lempke AF, Hart JM, Hryvniak DJ, Rodu JS, Hertel J. Use of wearable sensors to identify
416	biomechanical alterations in runners with Exercise-Related lower leg pain. Journal of
417	Biomechanics. 2021 Sep 20;126:110646.
418	34. Napier C, Menon C, Paquette MR. Session rating of perceived exertion combined with
419	training volume for estimating training responses in runners. Journal of Athletic Training. 2020
420	Dec 1;55(12):1285-91.
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