

1 **Rapid Force Generation during Unilateral Isometric Hamstring Assessment: Reliability**
2 **and Relationship to Maximal Force.**

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26 **Abstract**

27 Limited research has reported the reliability of rapid force generation characteristics during
28 isometric assessments of the hamstrings. Therefore, the purpose of the present study was to
29 determine the between-session reliability of rapid force generating characteristics of the
30 hamstrings and relationship to maximal force production. Twenty-three female soccer players
31 (age: 20.7 ± 4.7 years; height: 168.7 ± 5.9 cm; body mass: 64.4 ± 6.7 kg) performed three
32 unilateral trials of the 90-90 isometric hamstring assessment, on two separate occasions,
33 separated by 7-days. Peak force, force at 100- and 200 ms and average rate of force
34 development (aRFD) over 100- and 200ms epochs were calculated. Absolute and fair-good
35 reliability was observed for peak force and all rapid force generating measures ($<8.33\text{CV}\%$,
36 $\text{ICC}>0.610$). Significant and meaningful relationships ($p<0.001$, $r>0.802$) were observed for
37 all rapid force generating measures and peak force. The 90-90 isometric assessment can be
38 used to assess peak and rapid force generating reliably to enable practitioners to confidently
39 track changes in performance over time as part of fatigue monitoring and management.

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41 **Key words: female soccer, hamstring strength, force plates, fatigue monitoring**

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51 **Introduction**

52 Hamstring strain injuries (HSIs) remain one of the most prevalent non-contact muscular strain
53 injuries occurring within team sports (Brooks et al. 2006; Ekstrand et al. 2011; Ekstrand et al.
54 2016; Malone et al. 2018; Read et al. 2018; Roe et al. 2018; Panagodage Perera et al. 2019;
55 D'Alonzo et al. 2021). Soccer has one of the highest rates of HSI occurrence, which is partly
56 due to two of the primary proposed mechanisms of HSIs frequently occurring during match
57 play and training, i.e. kicking or high-speed running (Opar et al. 2012; Danielsson et al. 2020).
58 During high-speed running, for the hamstrings to resist the rapid knee extension during the
59 terminal swing phase (Chumanov et al. 2011), they are required to produce up to 10.5 N/kg
60 in resisted lengthening forces (Nagano et al. 2015). Heiderscheit and colleagues (2005)
61 approximated that a HSI event occurred at some point during the late swing phase or the very
62 initial stance phases with the earliest indication of an injury occurring only 0.1 s following foot
63 contact (Heiderscheit et al. 2005; Schache et al. 2009). Within professional soccer sprinting
64 based injuries occur most frequently during sprinting activities, specifically within the bicep
65 femoris long head (BF_{LH}) (Ekstrand, Bengtsson, et al. 2023). This observation highlights that
66 the ability for the hamstrings to produce extremely high forces rapidly is essential.

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68 A secondary cause of high rates of HSI incidence in soccer is generally a lack of compliance
69 to a known HSI prevention exercise (i.e. Nordic hamstring exercise (NHE)) (Bahr et al. 2015;
70 Ekstrand et al. 2022; Ekstrand, Hallén, et al. 2023), which has been shown to have a profound
71 effect on the successfulness of HSI prevention (Ripley et al. 2021). The implementation of the
72 NHE has been shown to increase proposed modifiable risk factors of HSI (Opar et al. 2012),
73 including BF_{LH} fascicle length and eccentric hamstring strength (Cuthbert et al. 2019). As a
74 modifiable risk factor for HSI eccentric hamstring strength was identified as a measure of
75 injury risk, with the Nordbord being used to identify risk (Opar et al. 2013; Bourne et al. 2015;

76 Opar et al. 2015; Timmins et al. 2016). However, more recently it has been established that
77 with team sports, pre-season eccentric hamstring strength testing provided minimal insight into
78 HSI incidence (Opar et al. 2021). Within the systematic review by Opar and colleagues (2021),
79 it was highlighted that more frequent follow up assessments could present different findings as
80 the studies included within the systematic review and meta-analysis follow up period was
81 between 3-10 months.

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83 As regular monitoring of hamstring strength could provide greater insight into potential HSI
84 risk, the ability to determine fatigue and decrements in performance will help practitioners
85 identify high risk occasions and adapt training to avoid potential injury sustainment (e.g.,
86 removal or limiting of high-speed running) (Opar et al. 2012). Following competitive and
87 simulated match play or repeated sprinting, eccentric hamstring strength has been shown to be
88 reduced (Greig 2008; Timmins et al. 2014; Matthews et al. 2017), however, as previously
89 identified the NHE is poorly adopted in team sports, hence other methods of monitoring
90 hamstring strength are required. Isometric hamstring strength assessments have been used to
91 identify changes in strength due to fatigue and HSI injury risk (McCall et al. 2015; Wollin et
92 al. 2016; Wollin et al. 2017, 2018; Constantine et al. 2019; Matinlauri et al. 2019; Bettariga et
93 al. 2023), with a variety of technologies, including externally fixed dynamometers and force
94 plates. With increasing availability of force plate technology, which can collect data and
95 provide instant feedback, force plate based isometric hamstring assessments are becoming
96 increasingly common, with several iterations but the most common being 90° of hip and knee
97 flexion (90-90°) (McCall et al. 2015; Constantine et al. 2019; Matinlauri et al. 2019; Cuthbert
98 et al. 2021; Bettariga et al. 2023). Despite the low association between isometric hamstring
99 assessments using force plates and eccentric hamstring strength measures (Moreno-Perez et al.
100 2020), the isometric assessments have been identified as sensitive enough to monitor fatigue,

101 with previously identified reliability and measurement error scores (4.34-11.0% coefficient of
102 variation, 0.698-0.95 (0.274-0.980) intraclass correlation coefficient (ICC) (95% confidence
103 intervals (CI) and 26.2-31.9 N minimal detectable difference) (McCall et al. 2015;
104 Constantine et al. 2019; Matinlauri et al. 2019; Cuthbert et al. 2021; Bettariga et al. 2023).
105 However, only a single study to date has included rapid force generation (e.g., rate of force
106 development (RFD)) (Bettariga et al. 2023), in male semi-professional soccer players.
107 Therefore, the purpose of the present study was to determine the between session reliability of
108 rapid force generating characteristics and identify any relationships between rapid and maximal
109 force production, in professional female soccer players. It was hypothesised that all measures
110 would be reliable with meaningful relationships between peak force and rapid force production.

111 **Materials and Methods**

112 **Participants**

113 Twenty-three female soccer players playing in the Women's Super League, all of whom had a
114 minimum of 2-years resistance training experience (age: 20.7 ± 4.7 years; height: 168.7 ± 5.9
115 cm; body mass: 64.4 ± 6.7 kg) volunteered to participate in the study. Participants were required
116 to have had no hamstring related injuries for ≥ 6 months prior to taking part. Organizational
117 consent was acquired prior to approaching the participants and all participants provided written
118 informed consent, or parental/guardian assent where required, to participate in the study.
119 Ethical approval was granted by the institutional ethics committee in accordance with the
120 declaration of Helsinki. α -priori sample size estimation suggested a minimum sample of 20
121 participants to achieve a minimum acceptable power of 80%, with no systematic differences
122 between repeated measures to achieve a target width of 0.35 based of 2 repeated measures
123 (Mokkink et al. 2022)

124 **Experimental design**

125 A repeated measures cross-sectional design was used to determine the reliability of isometric
126 hamstring strength assessment. Participants completed the tests prior to their normal training
127 day on two occasions 72 h apart. The familiarization session was carried out 48 h after a
128 competitive fixture, following their recovery day, with the testing session completed three days
129 after familiarization, allowing at least 48 h recovery prior to their next competitive fixture.

130 **90-90 Isometric hamstring**

131 The 90-90 isometric assessments were measured using a force plate (Kistler Type 9286AA:
132 Kistler Instruments Inc, Amherst, NY, USA), sampling at 1000 Hz and collected using Kistler's
133 BioWare software. Placed upon a wooden plyometric box at an appropriate height for each
134 participant using a goniometer, this was determined by participants lying in a supine position
135 with their knee at 90° of flexion, their heel resting on the box and their hip at an angle
136 appropriate to allow the lower shank to be parallel to the floor (i.e., 90°) (Figure 1). The test
137 was applied unilaterally with the non-testing leg being placed fully extended next to the box
138 and arms placed across the chest. Three trials for each leg were executed by the participants
139 driving their heel down into the force platform for 3–5 s following three submaximal trials,
140 similar to the previous isometric tests such as the isometric mid-thigh pull. Participants were
141 instructed to remain as still as possible, without initiating a movement for at least a 1-second
142 period before the instructions to pull to permit the calculation of limb weight and associated
143 force-time data including onset. Participants were required to repeat trials if their hips raised
144 off the ground which was determined by visual inspection or if a countermovement was
145 performed, the latter of which was detected through inspection of the force trace following
146 each repetition.

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Data analysis

Raw force-time data for each trial were analysed using a customized Microsoft Excel spreadsheet (version 2019, Microsoft Corp., Redmond, WA, USA). Peak force, force at 100- and 200 ms and average RFD (aRFD) from onset over a 100- and 200 ms epoch were calculated from the net force values (excluding limb weight established from the one-second initial weighing period) for each trial. Onset of force was identified as 5 standard deviations (SD) from the one second quiet period (Dos'Santos et al. 2017). The mean of the three trials was taken and used for further analysis.

Statistical analyses

All statistical analyses were conducted using SPSS for Windows version 26 (IBM SPSS Inc, Chicago, IL). Data is presented as the mean \pm SD. Normality was verified using the Shapiro-Wilk's test. An a priori alpha level was set at <0.05 . Absolute reliability was calculated using coefficient of variance (CV%) based off the sample SD and 95% CI, interpreted as $<5.00\%$, 5.00-9.99%, 10.00-14.99% and $>15\%$ as excellent, good, moderate, and poor, respectively. Relative reliability was assessed using two-way absolute agreement (3,1) intraclass correlation coefficients (ICC) (Shrout and Fleiss 1979; McGraw and Wong 1996; Kottner et al. 2011; Koo and Li 2016), ICC values were interpreted based on the lower bound CI (ICC; poor <0.49 , moderate 0.50–0.74, good 0.75–0.89 and excellent >0.90) as suggested by Koo & Li (2016). The standard error of measurement (SEM) and smallest detectable difference (SDD) for each variable were calculated to establish measurement error scores. The SEM was calculated using the following formula, where SD_{pooled} represents the pooled SD across the two testing sessions:

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$$SD_{Pooled} \times \sqrt{1 - ICC}$$

176 The SDD was calculated using the following formula:

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$$(1.96 \times \sqrt{2}) \times SEM$$

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179 Differences between testing sessions were evaluated using a series of t-tests, with Bonferroni
180 post hoc analysis. The magnitude of differences was also calculated using Cohen's *d* effect
181 sizes and interpreted based on the recommendations of Hopkins (2010) 0.00–0.19 = trivial and
182 0.20– 0.59 = small, >0.60 = moderate.

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184 Pearson's correlation coefficients (*r*) with 95% CI, coefficient of determination (*R*²) and
185 percentage of explained variance were calculated to determine if any relationships exist
186 between peak force and rapid force generating measures. Relationships between measures were
187 interpreted using Hopkins (2006) scale, 0-0.1, 0.11-0.30, 0.31-0.50, 0.51-0.70, 0.71- 0.9 and
188 >0.90, as trivial, small, moderate, large, very large and nearly perfect, respectively. All
189 Pearson's correlation coefficients (*r*) were corrected for familywise using Bonferroni
190 correction.

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192 **Results**

193 Good-excellent absolute and poor-moderate relative reliability was observed for all rapid force
194 generating measures (<8.33CV%, ICC>0.610), with excellent absolute and good relative
195 reliability was observed for peak force (2.84CV%, ICC=0.898) (Table 1).

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197 ****INSERT TABLE 1 ABOUT HERE****

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199 Significant and meaningful relationships ($p < 0.001$, $r > 0.802$) were observed between all force
200 generating measures, with stronger associations observed at 200ms (Figures [2](#) and [3](#)).

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202 Rapid force generating measures were able to explain >64% of peak force attained in the
203 isometric hamstring assessment (Figure [2](#) and [3](#)). Force at 200ms and aRFD over 200ms was
204 able to explain a greater percentage of variance in peak force, than both measures taken over
205 100ms.

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****INSERT FIGURE [2](#) ABOUT HERE****

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211 **Discussion and Implications**

212 The aims of the present study were to determine the reliability of peak force and rapid force
213 generating measures during a unilateral isometric hamstring assessment within female soccer
214 players and explore the relationships between peak force and rapid force generating measures
215 (force at 100- and 200 ms and aRFD over 100- and 200 ms). The results from this study
216 revealed that peak force and rapid force generating measures (specifically force at 100 ms and
217 200 ms) were reliable and could be longitudinally tracked, with only trivial to small differences
218 between sessions. Excellent absolute reliability and good relative reliability identified for peak
219 force, and good-excellent absolute reliability and poor-moderate relative reliability identified
220 for all rapid force generating measures, with poor relative reliability observed for aRFD over
221 100- and 200 ms. Statistically significant and very large relationships were identified between
222 all measures, in agreement with our hypothesis that stronger associations were seen at 200 ms
223 in comparison to 100 ms for force at set time points and aRFD.

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225 The findings of the present study are consistent with previous literature (McCall et al. 2015;
226 Constantine et al. 2019; Matinlauri et al. 2019; Cuthbert et al. 2021; Bettariga et al. 2023), with
227 good-excellent levels of reliability for peak force which could be used to track changes over
228 time either acutely with changes through fatigue, or chronically with changes due to training.
229 Within the present study, rapid force generating measures were found to be good-excellent
230 absolute reliability, albeit with only fair relative reliability, this is consistent with the results of
231 Bettariga et al. (2023) with moderate relative reliability also observed. Contrastingly, there was
232 poor absolute reliability identified in RFD between 50-100 ms and 100-150 ms (Bettariga et
233 al. 2023). It is crucial for variables to be determined as reliable and remain so over time,
234 especially for repeated measures which could highlight injury risk and potentially be used for
235 training adjustment as these could be impactful on an athlete or teams' success or athletic

236 potential. To achieve reliable measures, the methods need to be consistently applied, this
237 includes set up, instructions, data collection and data analysis, which may require standard
238 operating procedures designed and followed within a multi-disciplinary team.

239

240 The reliability observed within the present study for a single joint isometric assessment using
241 force plates is similar to what has been observed previously for multi-joint assessment of
242 isometric strength, with peak force having good-excellent test-retest reliability (Grgic et al.
243 2022). Similar to the present study, rapid force generating characteristics (force at set time
244 points and RFD) within the isometric mid-thigh pull have displayed lower levels of reliability
245 than peak force (Dos'Santos et al. 2017; Guppy et al. 2022), with measures of RFD possessing
246 lower reliability than force set time points (Dos'Santos et al. 2017; Guppy et al. 2022). This
247 similarity does present an interesting point which could be applicable for isometric hamstring
248 test used within the present study. If measures of RFD are less reliable than force at set time
249 points it is prudent for practitioners to be aware of this as this would impact on its useability
250 for fatigue monitoring, as large fluctuations in RFD could be expected due to biological error.
251 However, if force at 100- or 200 ms increases, RFD will have also increased but any change
252 will less likely be down to biological error. However, the sensitivity of all the rapid force
253 generating measures to fatigue requires further observation, as this will help determine their
254 usefulness to practitioners.

255

256 The present study also highlights that very large associations between peak force and rapid
257 force generating capacity were stronger at 200 ms in comparison to 100 ms for force at set time
258 points and aRFD, this is consistent with previous single joint literature observing stronger
259 explained variance with increases from the time of onset in knee extension based assessments
260 (Andersen and Aagaard 2006; Folland et al. 2014). This finding is also consistent with multi-

261 joint assessments, such as the isometric mid-thigh pull, whereby rapid force generating
262 measures at longer time periods (Comfort et al. 2019). The authors also suggested that
263 expressing early force production as a percentage of peak force could provide greater insight
264 into training adaptations and warrants further investigation (Comfort et al. 2019).

265

266 The present study is not without its limitations, firstly as discussed testing methods or standard
267 operating procedures should be carefully considered as one potential source of error could be
268 from wearing shoes, where the rubber sole may dampen a force response. Similarly, measures
269 may not be truly maximal if athletes are not secured to the ground, if trials are failed when hips

270 raise, or if there is an accurate representation of isometric hamstring force (or strength)?

271 Therefore, further research is required to explore these methodological aspects that could
272 change the observed results. Moreover, similar to the research in the isometric mid-thigh pull

273 (Dos'Santos et al. 2016; Dos'Santos et al. 2017), the methods used to analyse data collected can
274 impact the findings. Researchers should look to explore the effect of sampling frequency and
275 onset thresholds for isometric hamstring assessments including the 90-90 isometric assessment.

276 If a reliable and accurate onset threshold can be identified other than 5 x SD as used within the
277 present study, this could be imbedded within commercially automatic software which is now
278 frequently used by practitioners to provide rapid feedback.

279

280 Peak and rapid force generating measures can be collected using the 90-90 isometric
281 assessment within female soccer players reliably. The 90-90 isometric assessment could be
282 used by practitioners to effectively track changes in performance as part of a holistic
283 performance program and identify positive adaptations as a result of training. It could also be
284 used to monitor and inform practitioners of acute player fatigue; this could indicate the need
285 for intervention strategies and/or training manipulation. Training manipulation could come in

286 form of complete or partial removal from training to minimise the risk of HSI (Malone et al.
287 2018). However, a need for standardised methods for practitioners and further investigation on
288 the sensitivity of these measures to fatigue is required.

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290 **Word count - 4285**

291 **Data availability**

292 The data that support the findings of this study are available from the corresponding author,
293 [author initials], upon reasonable request.

294 **Disclosure statement**

295 No potential conflict of interest was reported by the authors.

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298

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Table 1. Between session mean, standard deviation (SD), absolute and relative reliability and absolute and relative (%) measurement error scores.

	Mean (SD)		Between session measures				
	Session 1	Session 2	Cohen's <i>d</i> effect size (95% CI)	CV% (95% CI)	ICC (95% CI)	SEM (%)	SDD (%)
Peak Force (N)	215.15 (44.16)	206.68 (46.66)	0.19 (-0.63;1.01)	2.84 (2.02;3.66)	0.898 (0.827;0.944)	1.91 (0.91)	5.29 (2.51)
Force at 100ms (N)	123.48 (34.52)	115.75 (39.38)	0.21 (-0.61;1.03)	4.57 (3.25;5.89)	0.784 (0.617;0.915)	3.07 (2.57)	8.51 (7.11)
Force at 200ms (N)	153.44 (39.22)	137.30 (42.59)	0.39 (-0.44;1.21)	7.38 (5.25;9.61)	0.770 (0.611;0.892)	6.25 (4.30)	17.32 (11.92)
aRFD over 100 ms (N/S)	1234.84 (345.17)	1097.50 (393.84)	0.37 (-0.46;1.19)	8.33 (5.92;10.74)	0.642 (0.463;0.787)	58.11 (4.98)	161.07 (13.81)
aRFD over 200 ms (N/S)	767.20 (196.12)	816.50 (212.95)	0.24 (-0.58;1.06)	4.40 (3.13;5.67)	0.610 (0.451;0.732)	18.77 (2.37)	52.03 (6.57)
SD = standard deviation, CV% = coefficient of variation percentage, ICC = intraclass correlation coefficient, SEM = standard effort of the measurement, SDD = smallest detectable difference. aRFD = average rate of force development.							

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476 Figure 1.

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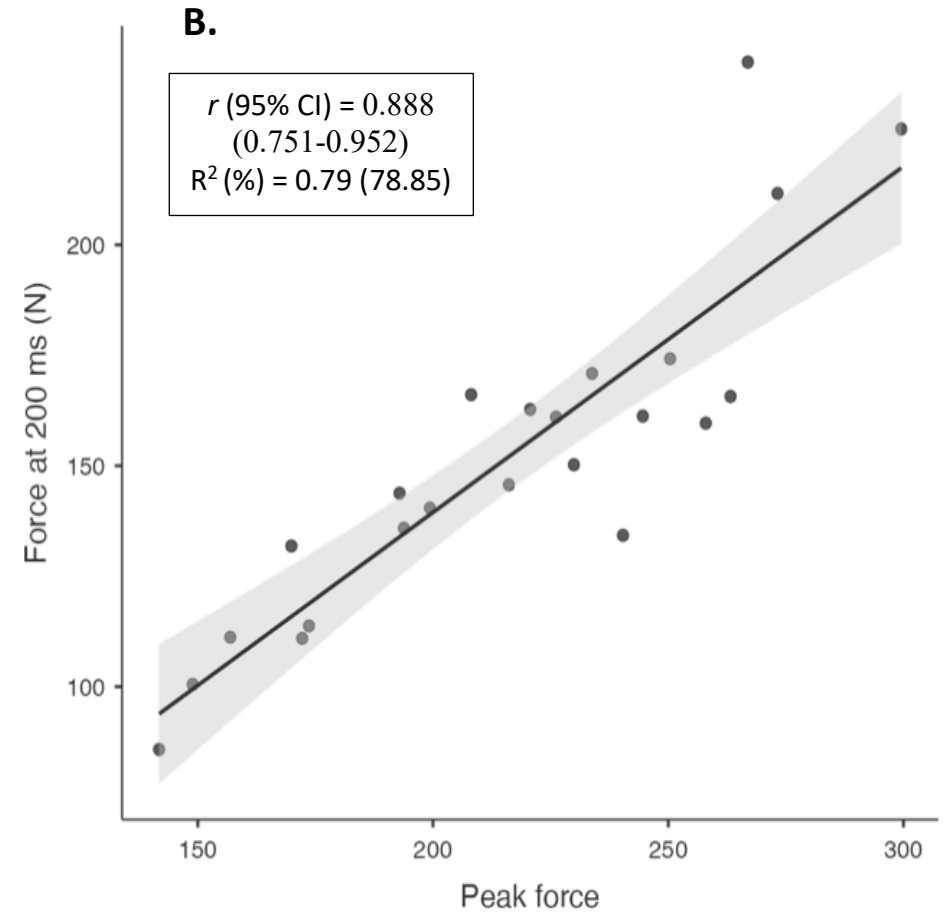
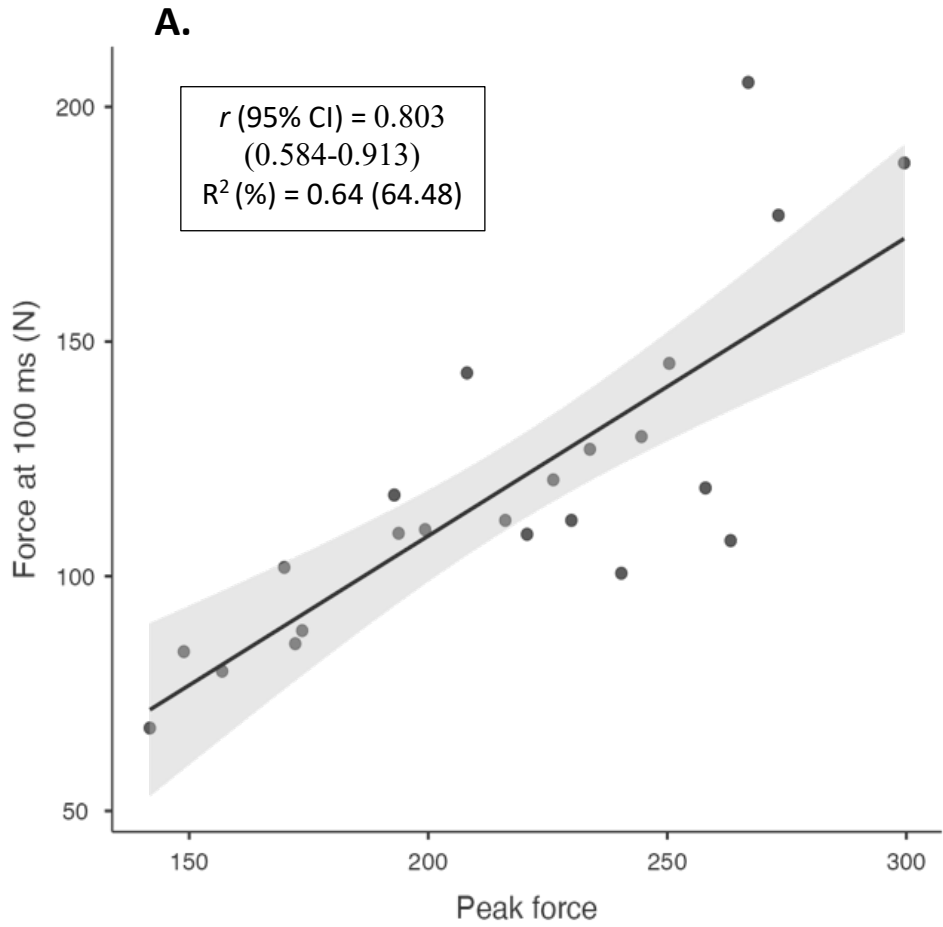


Figure 2 A & B.

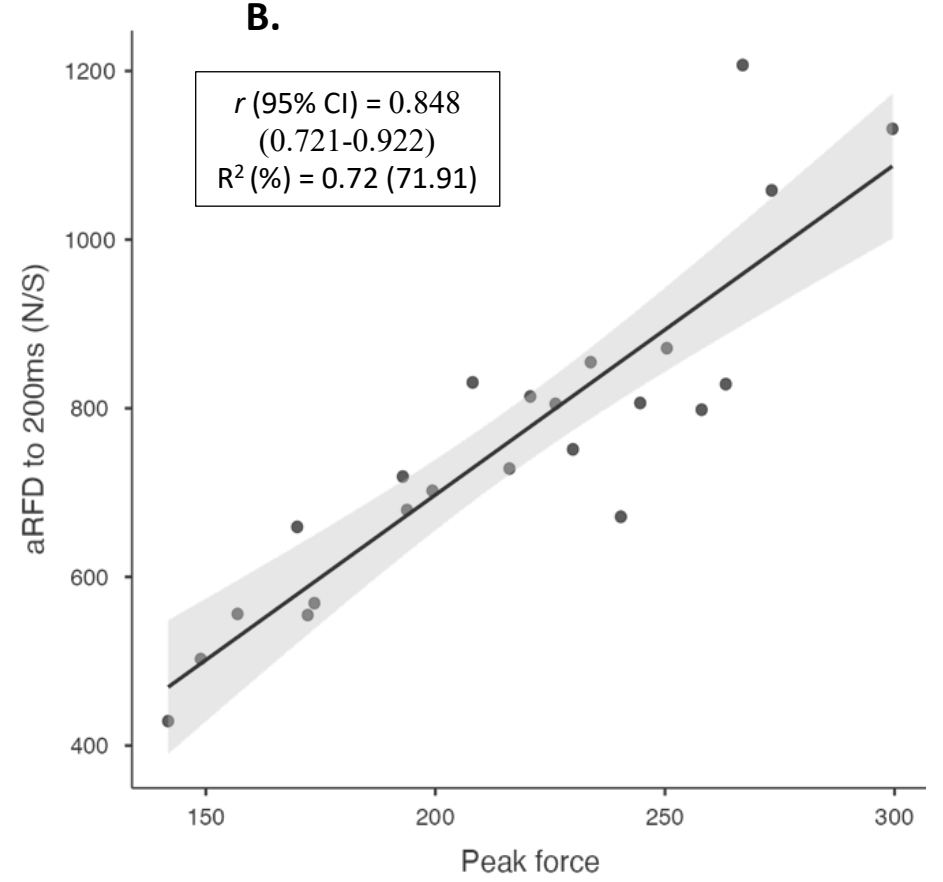
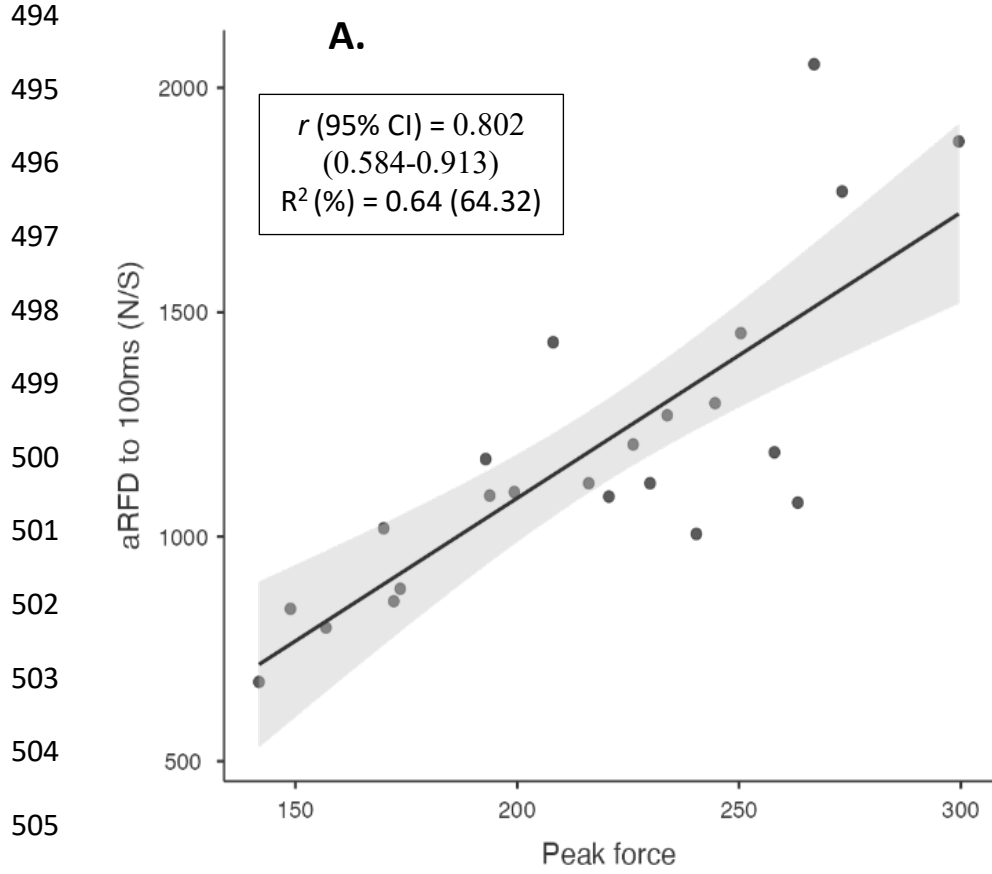


Figure 3 A & B.

510 Figure 1. Representation of the 90-90 isometric assessment.

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514 Figure 2 A & B. Scatterplots with linear trend line and 95% CI, Pearson's correlation
515 coefficient (r) with 95% CI and coefficient of determination (R^2) with percentage of
516 explained variance illustrating the relationship between peak force and A) force at 100 ms, B)
517 force at 200 ms.

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519 Figure 3 A & B. Scatterplots with linear trend line and 95% CI, Pearson's correlation
520 coefficient (r) with 95% CI and coefficient of determination (R^2) with percentage of
521 explained variance illustrating the relationship between peak force and A) aRFD over 100 ms
522 and B) aRFD over 200 ms.

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